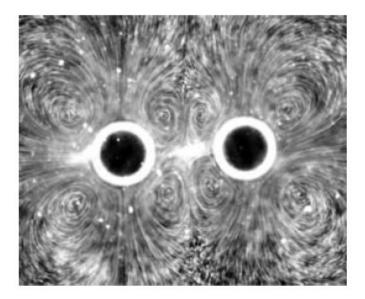


Fluid flows driven by sound and their applications

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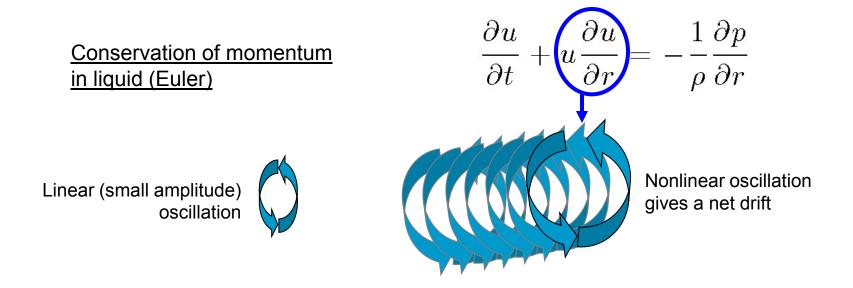


Co-authors

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1. Mean flows driven by fluid oscillations



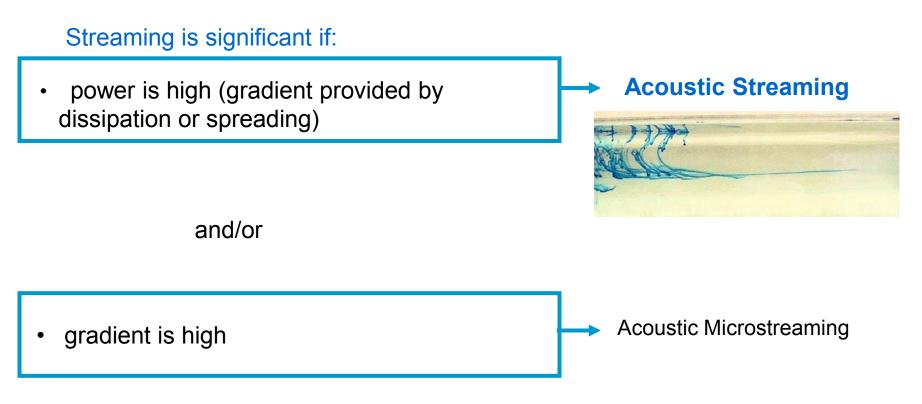
Any fluid will *rectify* oscillation, giving *mean streaming*

2nd order mean flow velocities are always much lower in magnitude than 1st order oscillatory flow velocities

But the mean flows *keep going*, so we can see them, unlike the oscillatory flows which cancel out

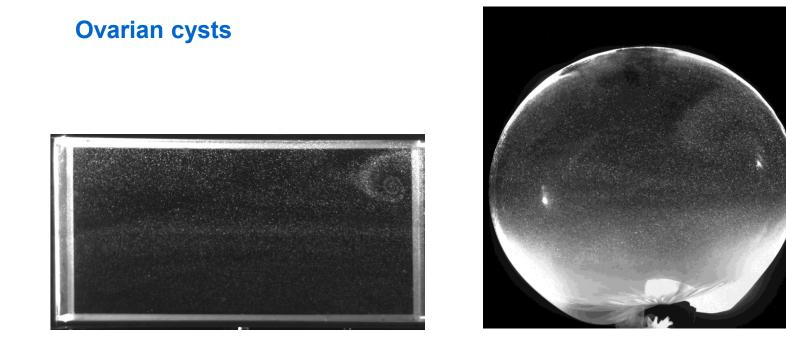
SWIN BUR * NE *

To create a net drift, the nonlinear term must exist. Thus, a **gradient** in the acoustic field must exist.



2. Acoustic Streaming



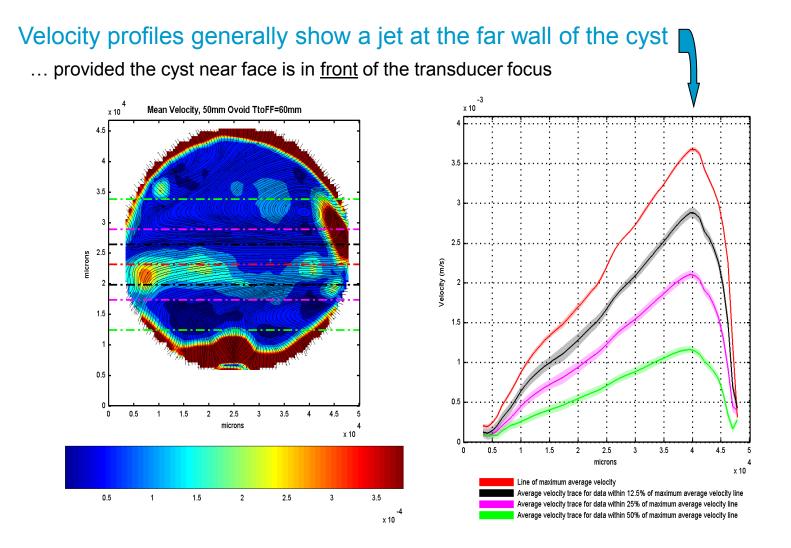


Experimental variations

- Regular geometric shapes of various types (cylinders, boxes) and ovoid shapes investigated
- Different sizes, aspect ratios and angles to the transducer beam were investigated 31 combinations, with dimensions ranging from a few mm to 12 cm

2.1. Acoustic Streaming in medical diagnostics







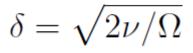
To create a net drift, the nonlinear term must exist. Thus, a **gradient** in the acoustic field must exist.

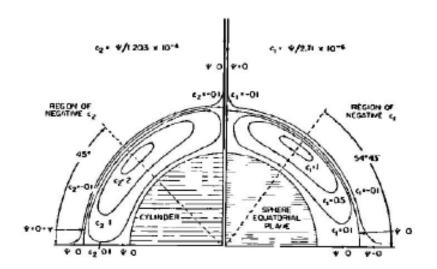
Streaming is significant if:



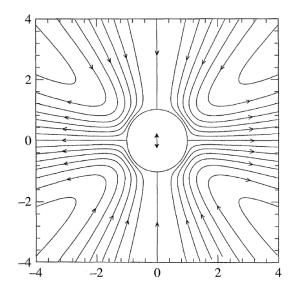
3.1. Acoustic microstreaming and bubbles

- Primary vortices: flow within the Stokes boundary or shear wave layer
- Secondary vortices flow outside boundary layer





Primary vortices Lane 1955, JASA 27, 1082



Secondary vortices Longuet-Higgins 1998, *Proc.RSL. A*, **454**, 72574

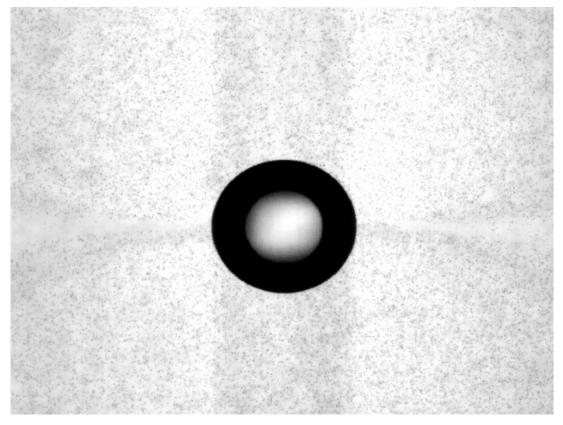


3.1. Acoustic microstreaming and bubbles



Cavitation microstreaming

- Acoustic microstreaming observed around oscillating bubbles
- The flow is observed as a system of vortices around the bubble

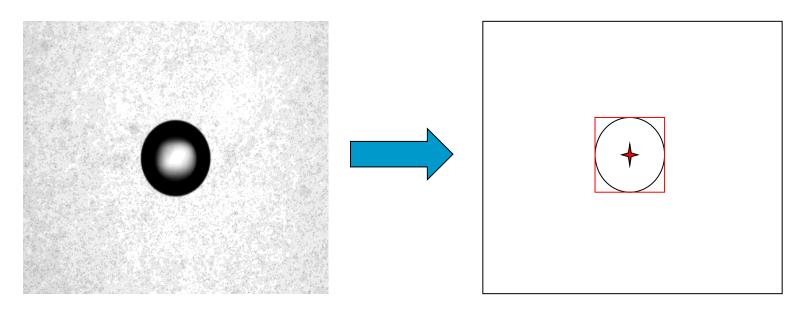


Tho, P., Manasseh, R., Ooi, A., 2007, J. Fluid Mech. 576, 191-233.



Measuring bubble motion

- Apply an edge detection algorithm to image of bubble
- Take binary image data and determine centroid of image and radius

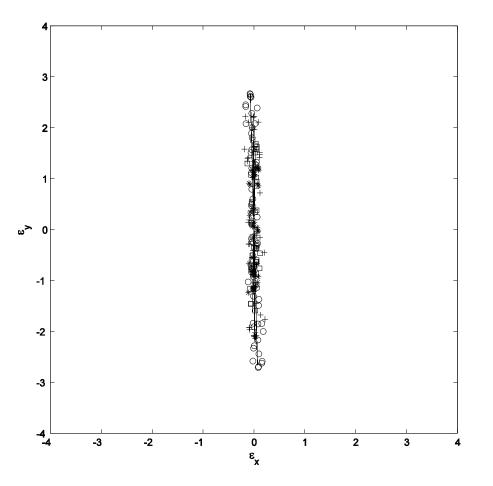


Tho, P., Manasseh, R., Ooi, A., 2007, *J. Fluid Mech.* 576, 191-233.

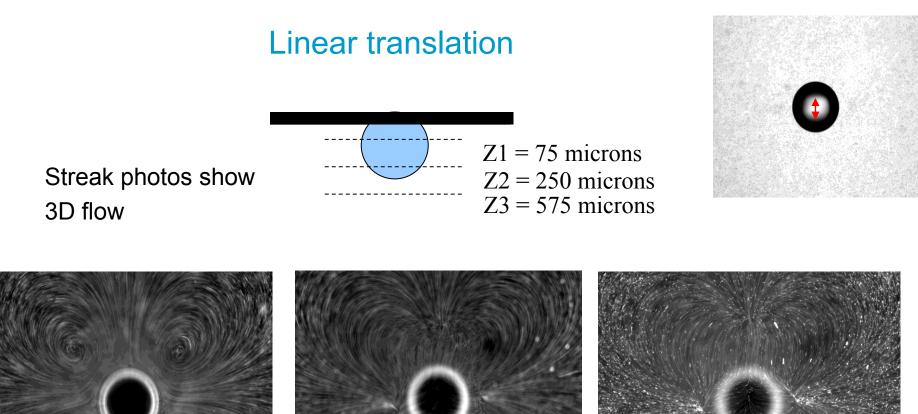
3.1. Acoustic microstreaming and bubbles



Linear translation

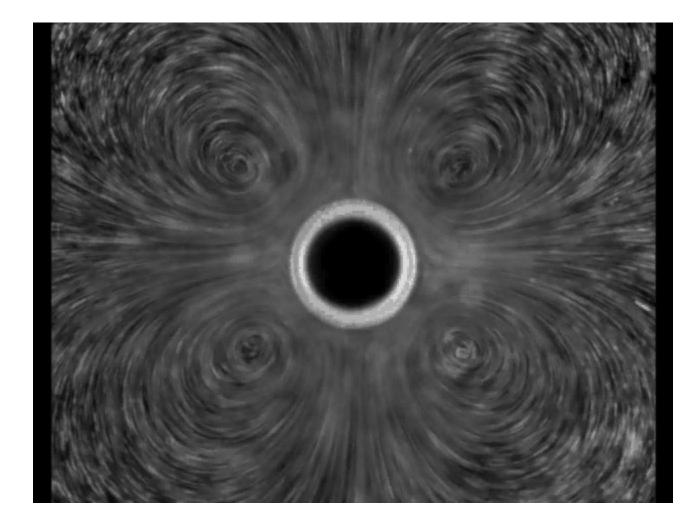






Tho, P., Manasseh, R., Ooi, A., 2007, J. Fluid Mech. 576, 191-233.

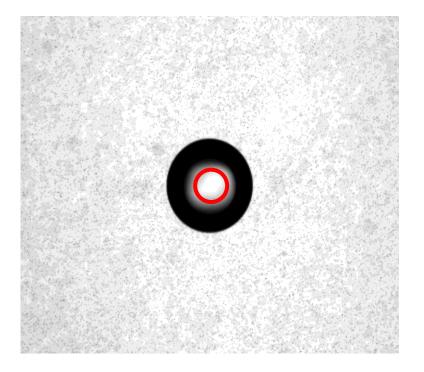




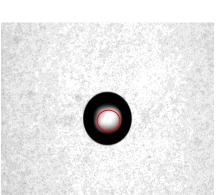


Circular orbit

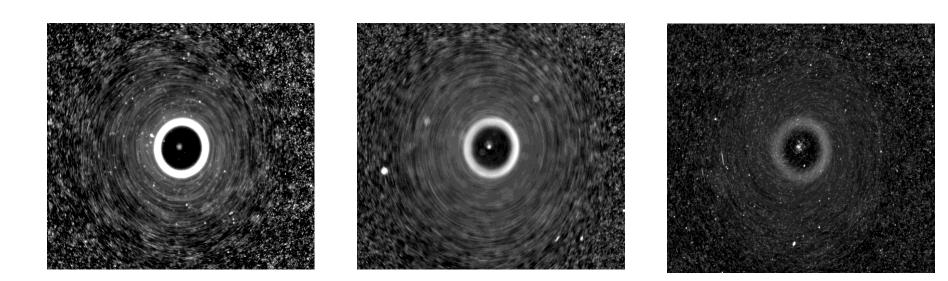
- A circular orbit
- Bubble moves in anticlockwise
 manner



Circular orbit



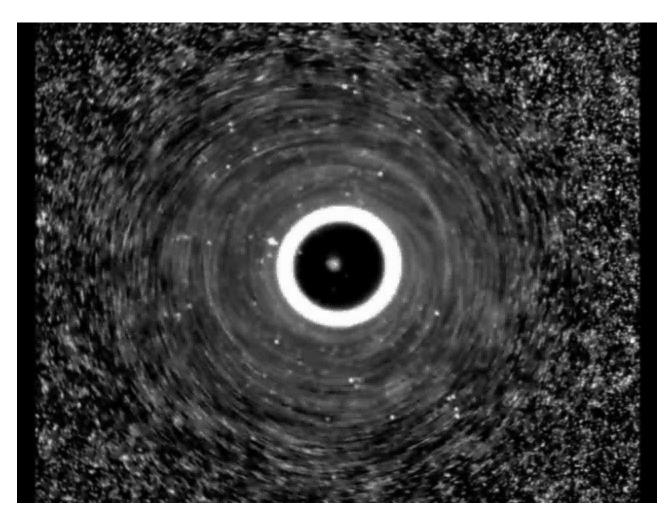
SWIN RI IR



Z1 = 75 microns

Z2 = 250 microns Z3 = 575 microns

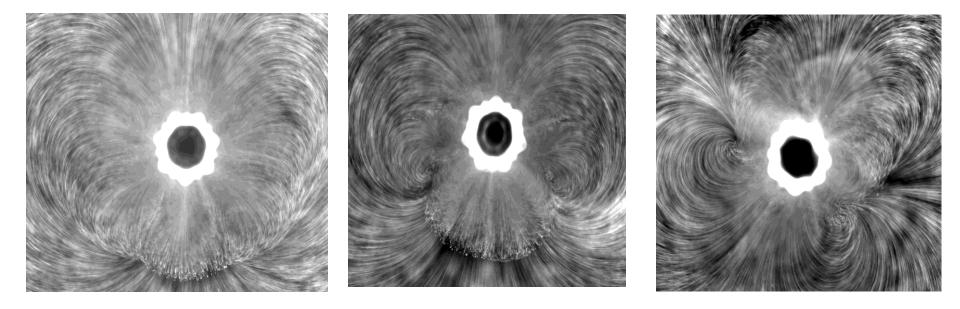




Tho, P., Manasseh, R., Ooi, A., 2007, J. Fluid Mech. 576, 191-233.

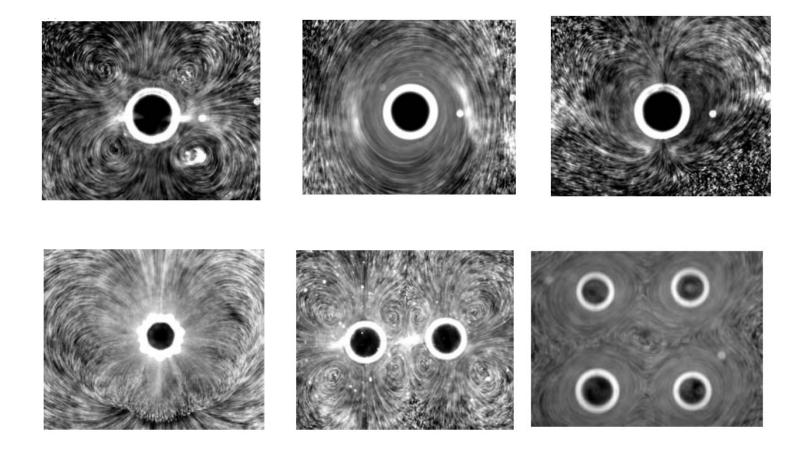


Shape modes





A variety of different flow patterns - streaklines



Tho, P., Manasseh, R., Ooi, A., 2007, *J. Fluid Mech.* 576, 191-233.

4. Microstreaming and micromixing



The need for chaos

- For molecules to react they must be brought into intimate contact
- Molecular diffusion is extremely slow; rate proportional to $1/L^2$.
- The regions of liquid containing reactants must be blended such that a short distance *L* separates them, permitting fast diffusion
- At macroscopic scales, turbulence rapidly lengthens interfaces, thinning *L*.
- But at microscopic scales, there is no turbulence!
- Liquids must be stirred

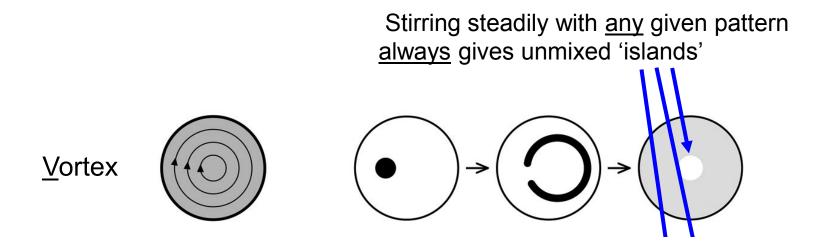
Petkovic-Duran, K., et al 2009, *Biotechniques* 47, 827-833.

Boon, et al 2011, Biotechniques 50, 116-119.

4.1. The micromixing problem



The need for chaos



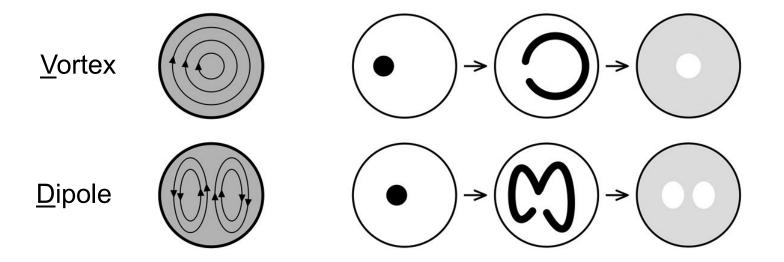
Petkovic-Duran, K., et al 2009, *Biotechniques* **47**, 827-833. Boon, et al 2011, *Biotechniques* **50**, 116-119.



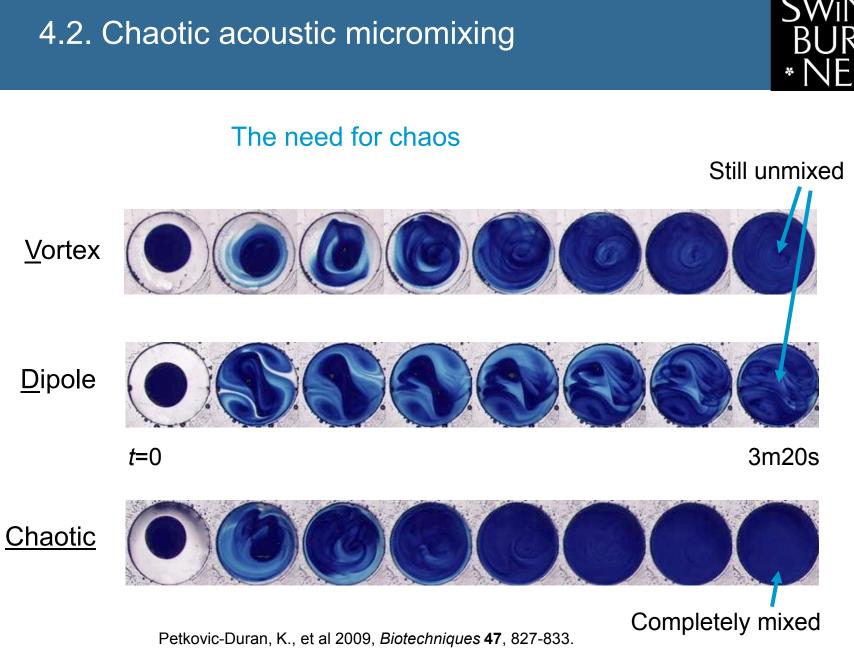
The need for chaos

Chaotic mixing theory states that to eliminate 'islands', patterns must that have mutually intersecting streamlines must be alternated with time:

$$\lor \to \mathsf{D} \to \mathsf{V} \to \mathsf{D} \to \mathsf{V} \to \mathsf{D} \to \mathsf{V} \to \mathsf{D} \to$$



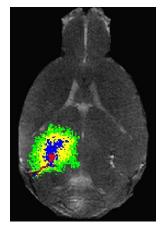
Petkovic-Duran, K., et al 2009, *Biotechniques* **47**, 827-833. Boon, et al 2011, *Biotechniques* **50**, 116-119.



Boon, et al 2011, *Biotechniques* **50**, 116-119.

5. Medical therapeutics with microbubbles

- Sonoporation is when molecules (DNA, drugs) that would not normally enter cells are found to enter and deliver benefit (gene therapy, chemotherapy) under the action of ultrasound
- Sonothrombolysis is when dangerous blood clots are dissolved or broken up under the action of ultrasound
- Both sonoporation and sonothrombolysis are improved when microbubbles are present



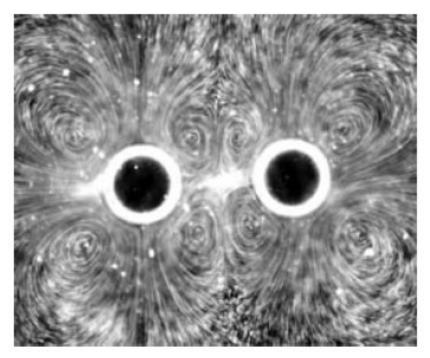
• Why?

Collis et al 2010 Ultrasonics 50, 273–279



There are *speculations* that *microstreaming* around microbubbles creates appropriate stresses on cells, or the extracellular matrix, to cause sonoporation or sonothrombolysis

Perren et al 2008, *J. Thromb Thrombolysis*, **25**, 219-223; Liu & Wu 2009, *JASA.* **125**, 1319-1330; Collis et al 2010 *Ultrasonics* **50**, 273–279



Tho et al 2007, J. Fluid Mech. 576, 191-233.

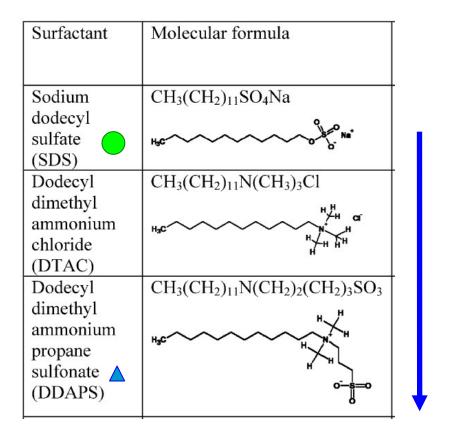
- Can we understand these bioeffects?
- Can we control them?



•Measure microstreaming velocities quantitatively, using microPIV, in the presence of different surfactants: SDS, DTAC, DDAPS

•Surfactant concentrations adjusted to give the **same surface tension**,50+/1 mN/m, irrespective of surfactant type

•Can we affect microstreaming velocities significantly by altering surfactant type?



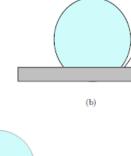
Increasing headgroup size

Bubbles

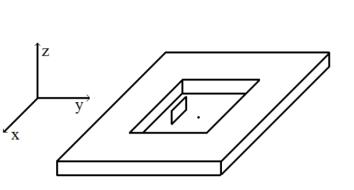
- Single bubbles, pendant (bottom and side)
- Formed by syringe
- 30 400 µm in diameter

Microchamber & transducer

- 35 mm x 30 mm x (1 or 3) mm
- Additional wall to view bubble side on
- Transducer mounted onto cover
- 28 kHz CW



Bubble



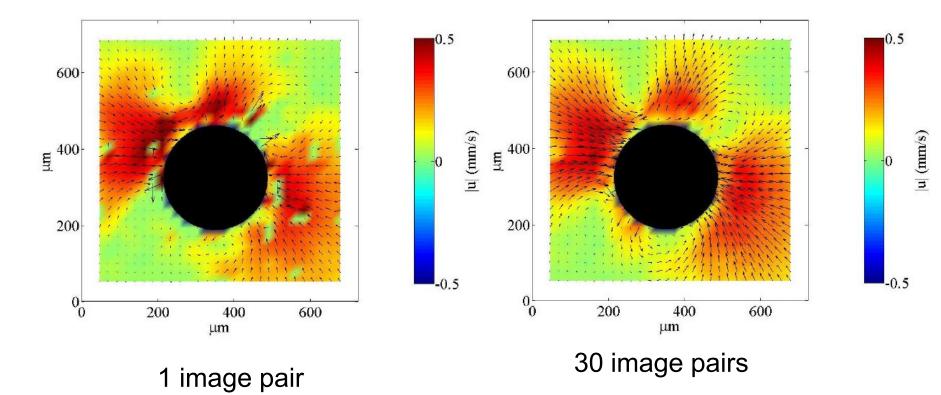
Plane wall



Plane

wall

The PIV image pair were averaged over the data set to remove outliers and anomalies from the PIV analysis (30 – 200 image pairs)





Divergence metric

The **divergence** in the *x*-*y* plane measured closest to the wall was calculated

$$\nabla U_{\mathbb{W}} = \begin{pmatrix} \partial & \partial \\ \partial & + \nu \\ \partial & - + \nu \\ \partial & \partial \\ \mathcal{X}_{\mathbb{W}} & \mathcal{Y}_{\mathbb{W}} \end{pmatrix}$$

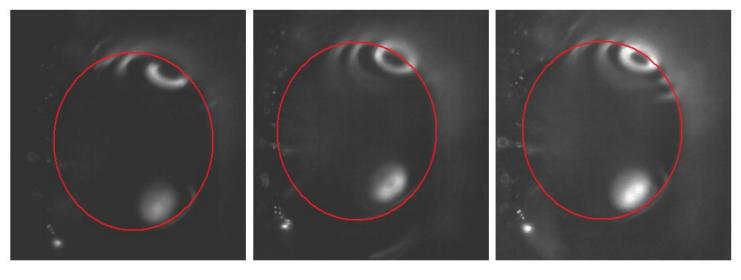
Propose that divergence represents the stretching or compression of a cell membrane or tissue surface that the bubble is affecting

The traditional biomedical measure is shear stress, but this is in a plane at right angles to the affected surface

Collis et al 2010 *Ultrasonics* **50**, 273–279



 Velocity = 13 ± 2 mm/s, two orders of magnitude greater than secondary velocity



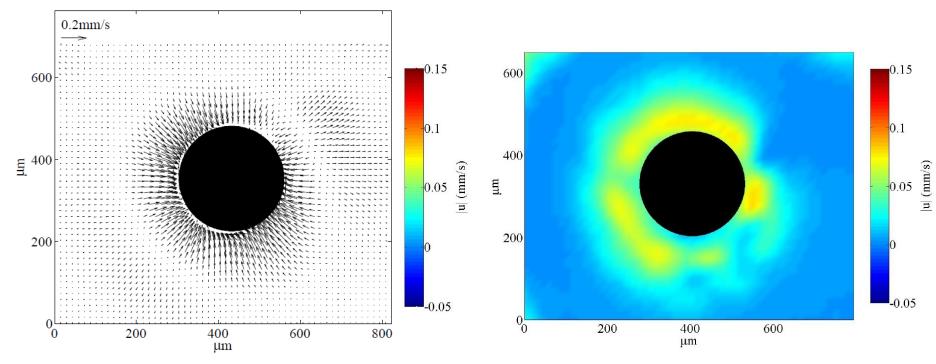
(a) (b) (c)

A 270 μ m bubble excited at f = 28 kHz, amplitude = 20 V_{p-p} and captured in the X-Z plane with varying exposure to estimate the velocity of primary vortices at a speed of $13.35 \pm 2 \text{ mms}^{-1}$ a) exposure time of 5884 μ s, b) exposure time of 8322 μ s c) exposure time of 11767 μ s



Surfactant: DDAPS

Surfactant: SDS

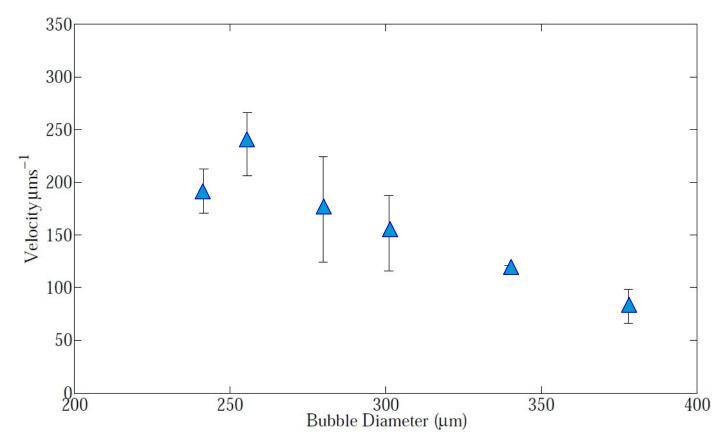


Velocity magnitude, bubbles driven at 28 kHz, 4.1 kPa

Recall the surface tension is the same (within 2%) only the type of molecule is different



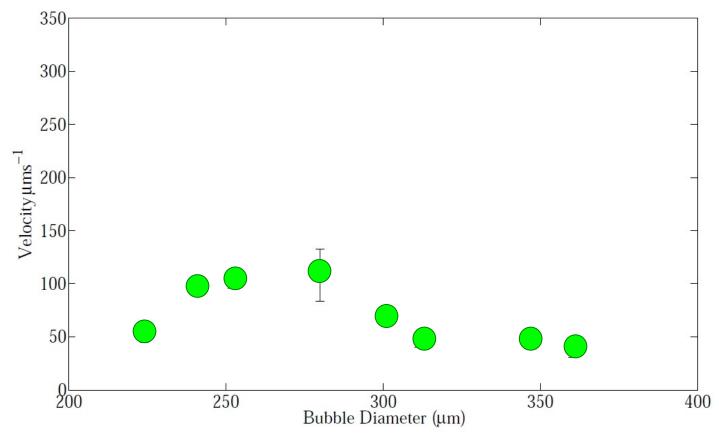
Surfactant: DDAPS



Maximum microstreaming velocities, bubbles driven at 28 kHz, 4.1 kPa

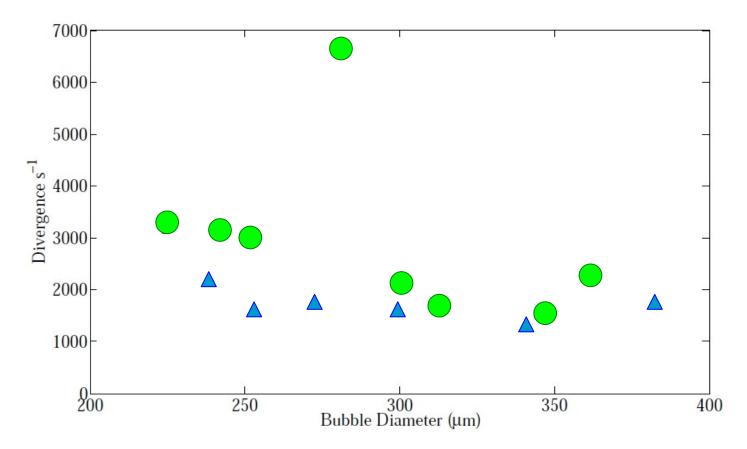


Surfactant: SDS



Maximum microstreaming velocities, bubbles driven at 28 kHz, 4.1 kPa

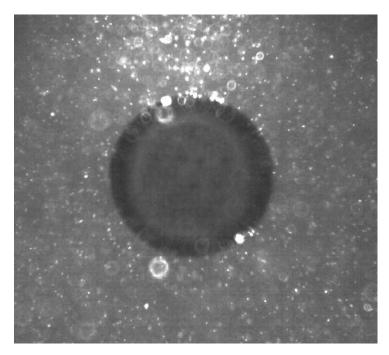




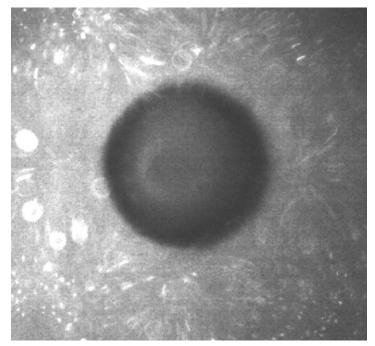
Max Divergence in the *x*-*y* plane, bubbles driven at 28 kHz, 4.1 kPa



Threshold effect under identical physical and imaging conditions



Water: low velocities



DTAC: high velocities, surface instabilities

Leong et al 2011, *J. Phys. Chem. C* **115**, 24310





- 1. Fundamental nonlinearities create steady fluid flows when sound is applied: streaming and microstreaming
- 2. **Streaming** can be used for medical **diagnostics**
- 3. Microstreaming can occur in a variety of patterns
- 4. Microstreaming can be used for fluid mixing and may be relevant to new medical therapeutics
- 5. Even when the surface tension is maintained the same, surfactants with different molecular head groups create very different microstreaming velocities